Electrode Configurations for Piezoelectric Tube Actuators With Improved Scan Range and Reduced Cross-Coupling

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Abstract—The article describes two new methods for driving piezoelectric tube scanners. The first method aims to maximize horizontal and vertical scan range by driving the internal electrode rather than grounding it. This approach eliminates the need for a circumferential Z-electrode, which permits longer quadrant electrodes that develop greater deflection and vertical scan range. Experimental results demonstrate a 62% increase in lateral scan range and an 87% increase in vertical scan range. The second method aims to eliminate mechanical cross-coupling between the lateral deflection, tilt angle, and vertical extension. This method involves splitting the piezoelectric tube into eight external electrodes and a driven internal electrode, similar to the first method. This configuration results in less lateral deflection but significantly reduces the tilting and vertical motion induced by lateral deflection. Experimental results demonstrate a 44% increase in vertical displacement, 96% reduction in tilting, and 62% reduction in vertical cross-coupling.

Index Terms—Actuator, nanopositioning, piezoelectric tube.

I. INTRODUCTION

PIEZOELCTRIC tube actuators are monolithic nanopositioning devices which are mechanically simple and compact. They are available at a much lower cost compared to other positioning stages such as flexure-guided nanopositioners [1]–[7]. When used as a nanopositioner, piezoelectric tubes are capable of motion in two lateral axes (X- and Y-axes) and vertical motion (Z-axes). Rotational and angular motion requires a flexure-based structure [8]. The simplicity and low cost of piezoelectric tube actuators have made them common in applications such as fiber-optic scanning [9], [10], endoscopic imaging [10]–[12], two-photon microscopy [13], [14], and atomic force microscopy [6], [15]–[17]. The schematic of a conventional tube actuator with quartered electrodes is shown in Fig. 1(a).

The piezoelectric tube actuator is a thin-walled cylinder of radially poled piezoelectric ceramic. For XYZ positioning, the standard configuration uses four external quartered electrodes and a single circumferential Z-electrode, as shown in Fig. 1(a). The internal electrode is grounded. One end of the tube is fixed and the other end is free. When voltages with equal magnitude but opposite polarity are applied to a pair of opposite quartered electrodes, e.g., +200 and −200 V, one side of the tube extends while the opposite side contracts, resulting in bending and lateral deflection. The magnitude of bending is approximately proportional to the applied voltage [16]. Similarly, the other pair of electrodes provide actuation in the orthogonal direction. To displace in the Z-direction, voltage is applied to the circumferential Z-electrode which is conventionally one-third of the tube length and located at the free-end of the tube.

This article proposes an alternative configuration method actuation where the internal electrode is driven with a negative voltage (Vᵢ) rather than connecting it to ground. This approach eliminates the need for a circumferential Z-electrode which simultaneously allows longer quadrant electrodes, and allows the entire tube length to generate vertical displacement. To avoid exceeding the coercive field strength of the material, the internal voltage is restricted to a negative polarity. It should be noted that the maximum electric field in the poling direction is doubled by the proposed method. However, this is typically five times the coercive field strength; so the resulting electric field is less than half of the limiting value. The proposed actuation method is applied to a piezoelectric tube with full-length quartered electrodes as shown in Fig. 1(b).

A disadvantage of the standard drive method described above is tilting of the moving platform which is proportional to deflection. The tilt angle distorts the interference pattern in optical microscopy [18] and reduces image quality in atomic force microscopy [19]. To reduce the tilt angle, an eight-electrode tube actuator is proposed where the outer electrodes are split to create upper and lower sections. When applying voltages with the same magnitude on the X- or Y-electrode but with opposite polarity at the two halves, the tube bends in a sigmoid shape which reduces the tilt angle significantly. However, the deflection range is approximately halved, as described in Section II-B. In [19],
Fig. 1. Electrode configuration and driving method for the (a) conventional, (b) full-length, and (c) eight-electrode piezoelectric tube actuators.

Fig. 2. Cross-section of the tube in the $XY$ plane. The $Y$-electrodes are driven with equal but opposite voltages $V_y$, and the internal electrode is driven by $V_i$. The $X$-electrodes are grounded.

configuration shown in Fig. 1(a). All three tubes have identical dimensions, that is, 50.8 mm length, 0.66 mm thickness, and an 9.5 mm outer diameter.

The rest of this article is organized as follows. Section II presents a detailed deflection analysis of the full-length and eight-electrode piezoelectric tubes. The modeling also establishes that the voltage $V_i$ applied to the inner electrode only affects vertical displacement. Section III compares the finite-element (FE) simulations of each configuration using ANSYS. Experimental results are presented and compared in Section IV. Section V concludes this article.

II. ANALYTICAL DEFLECTION ESTIMATIONS

A. Full-Length Piezoelectric Tube Actuator

This section derives the deflection of the full-length tube, as described in Fig. 1(b), based on the Euler–Bernoulli equations. To produce lateral deflection along the $Y$-axis, the $Y$-electrodes are driven differentially with $\pm V_y$ Volts as shown in Fig. 2. The $X$-electrodes are grounded and the internal electrode is actuated with $V_i$ Volts. Lateral deflection along the $X$-axis can be derived similarly by applying differential voltages to the $X$-electrodes.

In the following, polar co-ordinates $(z, r, \theta)$ are employed for convenience. The transformation $(x, y) = (-r \cos \theta, -r \sin \theta)$ converts Cartesian co-ordinates to polar co-ordinates. In the polar co-ordinates, the applied voltage $V(\theta)$ is

$$V(\theta) = \begin{cases} 
-V_y - V_i & \theta \in (\pi/4, 3\pi/4) \\
V_y - V_i & \theta \in (5\pi/4, 7\pi/4) \\
0 & \text{otherwise}
\end{cases} \quad (1)$$

Applying Euler–Bernoulli kinematic assumptions [20], the strain $S_1$ is

$$S_1(z, r, \theta) = -r \sin(\theta) \frac{d^2w}{dz^2} \quad (2)$$

where $(z, r, \theta)$ are cylindrical co-ordinates and $w(z)$ is the lateral deflection as a function of $z$. In this problem the tube is assumed thin and thus $r$ is the tube’s outer radius. In the Euler–Bernoulli beam, all other strains are zero. The constitutive equations of the piezoelectric material are

$$T_1 = ES_1 - e_{31}E_3 \quad (3)$$
\[ D_3 = \varepsilon_{31} S_1 + \varepsilon_{33} E_3 \]  

(4)

where \( T_1 \) is the stress, \( E \) is the elastic modulus, \( \varepsilon_{31} \) is the piezoelectric coefficient, \( E_3 \) is the electric field, \( D_3 \) is the electric displacement, and \( \varepsilon_{33} \) is the permittivity. Assuming a thin tube structure, the electric field is a function of voltage given by

\[ E_3 = V(\theta)/h \]

(5)

where \( h \) is the thickness of the tube. Substituting (2) and (5) into (3) results in the following expression for the stress around the circumference of the tube

\[ T_1 = -E\kappa \sin(\theta) w''(z) - \varepsilon_{31} V(\theta)/h. \]  

(6)

The first part of this expression is the stress caused by the mechanical structure and the second part is the stress due to the piezoelectric effect. These stresses induce moments which cause the cross-sectional area to rotate around the neutral axis. Assuming there is no net axial force on the structure, the total moment on the cross-sectional area is

\[ M = \int_0^{2\pi} y T_1 d\theta \]  

(7)

where \( y = -r \sin(\theta) \) as shown in Fig. 2. Substituting (1) and (6) into (7) gives,

\[ M = \int_0^{2\pi} -r \sin(\theta) T_1 d\theta \]

\[ = \int_\pi/4^{\pi/4} E\kappa^2 w''(z) d\theta \]

\[ + \int_{-\pi/4}^{3\pi/4} E\kappa^2 w''(z) + \varepsilon_{31}\kappa \left( -V_y - V_i \right) \right] d\theta \]

\[ + \int_{-\pi/4}^{5\pi/4} E\kappa^2 w''(z) d\theta \]

\[ + \int_{-\pi/4}^{7\pi/4} E\kappa^2 w''(z) + \varepsilon_{31}\kappa \left( \frac{V_y - V_i}{h} \right) \right] d\theta \]  

(8)

where \( \kappa = r \sin(\theta) \). Solving the above integration gives

\[ M = Er^2 w''(z)\pi + \frac{\sqrt{2E\kappa}}{h}\left( -V_y - V_i - V_y + V_i \right) \]

\[ = Er^2 w''(z)\pi - \frac{2\sqrt{2E\kappa} V_y}{h} \]  

(9)

Note that the voltage of the inner electrode \( (V_i) \) is eliminated in the above expression, indicating the internal driving voltage has no effect on the lateral deflection of the tube. With no external load, the net moment is zero when in equilibrium, that is

\[ M = Er^2 w''(z)\pi - \frac{2\sqrt{2E\kappa} V_y}{h} = 0. \]  

(10)

Rearranging the above equation and substituting \( r = D/2 \) and \( \varepsilon_{31} = Ed_{31} \) gives

\[ w''(z) = -\frac{2\sqrt{2E\kappa} V_y}{h D \pi} \]  

(11)

B. Eight-Electrode Piezoelectric Tube Actuator

The eight-electrode tube is also modeled using Euler–Bernoulli beam theory. To develop deflection along the \( y \)-axis, the upper and lower pairs of the quartered \( Y \)-electrodes are actuated with \( \pm V_y \) Volts and the internal electrode is actuated with \( V_i \) Volts as described in Fig. 3. The \( X \)-electrodes are grounded.
The voltage $V(z, \theta)$ applied is

$$V(z, \theta) = \begin{cases} -V_y - V_i, & \theta \in \left( \frac{\pi}{4}, \frac{3\pi}{4} \right), \quad z < \frac{L}{2} \\ V_y - V_i, & \theta \in \left( \frac{3\pi}{4}, \frac{5\pi}{4} \right), \quad z < \frac{L}{2} \\ V_y - V_i, & \theta \in \left( \frac{5\pi}{4}, \frac{7\pi}{4} \right), \quad z > \frac{L}{2} \\ -V_y - V_i, & \theta \in \left( \frac{7\pi}{4}, \frac{9\pi}{4} \right), \quad z > \frac{L}{2} \\ 0, & \text{otherwise} \end{cases}$$

For a thin tube, a parallel plate capacitive structure is used to approximate the electric field distribution in the tube. The radial electric field $E_3(z, r, \theta) = V(z, \theta)/h$, where $h$ is the thickness of the tube. Applying Euler–Bernoulli kinematic assumptions [20], the strain is

$$S_1(z, r, \theta) = -r \sin(\theta) w''(z) \quad (17)$$

where $w(z)$ is the lateral deflection. Due to the split in the outer electrode at $z = \frac{L}{2}$, $w''(z)$ is evaluated for the upper and lower sections separately

$$w''(z) = \begin{cases} w''_u(z) & z \in (0, \frac{L}{2}) \\ w''_d(z) & z \in (\frac{L}{2}, L) \end{cases} \quad (18)$$

Substituting $E_3(z, r, \theta)$ and $S_1(z, r, \theta)$ into (3) results in (19) for the following expression for the stress in the tube

$$T_1(z, r, \theta) = -E r \sin(\theta) w''(z) - e_{31} V(z, \theta)/h. \quad (19)$$

The first term of this expression is the stress exerted by the material, and the second term is the stress due to the piezoelectric effect. These stresses induce moments about the neutral axis of the tube. The total moment on the cross-sectional area is zero when in equilibrium and is evaluated in the upper and lower sections as

$$M_1(z) = Er^2 w''_u(z) \pi - \frac{2\sqrt{2} e_{31} r V_y}{h} = 0 \quad (24)$$

$$M_2(z) = Er^2 w''_d(z) \pi + \frac{2\sqrt{2} e_{31} r V_y}{h} = 0. \quad (25)$$

Rearranging and substituting $r = D/2$ and $e_{31} = Ed_{31}$, where $D$ is the diameter, and $d_{31}$ is the piezoelectric strain constant, the above equations give

$$w''_u(z) = \frac{4\sqrt{2} d_{31} V_y}{h D \pi}, \quad w''_d(z) = -\frac{4\sqrt{2} d_{31} V_y}{h D \pi}. \quad (26)$$

Integrating $w''_u$

$$w_1(z) = \phi_1(z) = K z + C$$

$$w_1(z) = \frac{z^2 K}{2} + C_1 z + C_2 \quad (27)$$

where $K = 4\sqrt{2} d_{31} V_y/(h D \pi)$ and $\phi_1(z)$ is the angle. Applying boundary conditions $w_1(0) = 0$ and $w_1(L) = 0$ results in $C_1 = 0$ and $C_2 = 0$. Similarly integrating $w''_d$ gives

$$w_2(z) = \phi_2(z) = -K z + C_3$$

$$w_2(z) = -\frac{z^2 K}{2} + C_3 z + C_4. \quad (28)$$

Applying boundary conditions $w_1(L) = w_2(L)$ results in $C_3 = KL$ and $C_4 = -K L^2/4$. Substituting these constants into $w_2$, the deflection of the eight-electrode tube actuator at $z = L$ is

$$\delta_y = w_2(L) = \frac{\sqrt{2} d_{31} L^2 V_y}{\pi Dh}. \quad (31)$$

That is, the deflection of the eight-electrode configuration is half that of the four-quadrant configuration [21]. This is the tradeoff required to eliminate tilting and cross-coupling. Similarly, the deflection equation in the X-axis is

$$\delta_x = \frac{\sqrt{2} d_{31} L^2 V_x}{\pi Dh}. \quad (32)$$

For vertical motion, the standard axial extension equation is

$$\delta_z = \frac{d_{31} L V_i}{h} \quad (33)$$

where $V_x$, $V_y$, and $V_i$ are the magnitudes of electrode voltages for the X-, Y-, and Z-axis, respectively. In the experimental setup, the voltages $V_x$ and $V_y$ are kept in the range [−200, 200] and $V_i$ is in the range [−200, 0]. Analytical deflections of the conventional, full-length, and eight-electrode tubes calculated using (12)–(13) and (31)–(33) are provided in Table III.

III. FINITE-ELEMENT ANALYSIS

A FE analysis is performed to compare the maximum deflection $\delta_z$, $\delta_x$, cross-coupling from X to $\phi$, and cross-coupling from X to $d_z$, of each electrode configuration. All three tubes are made of PZT-5H piezoelectric ceramic material having length
FE simulated deflections (in μm) and tilt angle (in μrad) of the (a) conventional, (b) full-length, and (c) eight-electrode piezoelectric tube actuators.

**TABLE I**
PIEZOELECTRIC PROPERTIES OF THE TUBE ACTUATORS

<table>
<thead>
<tr>
<th>Piezoelectric coeff. (C/m²)</th>
<th>Relative permittivity εᵣ/ε₀</th>
<th>Piezoelectric const. (×10⁻¹² m/N)</th>
</tr>
</thead>
<tbody>
<tr>
<td>εₓ₁</td>
<td>εₓ₁</td>
<td>ε₁₁</td>
</tr>
<tr>
<td>-53.3</td>
<td>23.3</td>
<td>17.0</td>
</tr>
</tbody>
</table>

**TABLE II**
VOLTAGES APPLIED TO THE FE MODELS TO DEVELOP LATERAL AND VERTICAL DEFLECTION

<table>
<thead>
<tr>
<th>Tube</th>
<th>Def.</th>
<th>Vₓ+/−</th>
<th>Vᵧ+/−</th>
<th>V₁</th>
<th>V₂</th>
</tr>
</thead>
<tbody>
<tr>
<td>Conventional</td>
<td>δₓ</td>
<td>±200</td>
<td>0</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>Conventional</td>
<td>δₓ</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>±200</td>
</tr>
<tr>
<td>Full-length</td>
<td>δₓ</td>
<td>±200</td>
<td>0</td>
<td>N/A</td>
<td>N/A</td>
</tr>
<tr>
<td>Full-length</td>
<td>δₓ</td>
<td>0</td>
<td>0</td>
<td>−200</td>
<td>N/A</td>
</tr>
<tr>
<td>Eight-electrode</td>
<td>δₓ</td>
<td>±200</td>
<td>0</td>
<td>N/A</td>
<td>N/A</td>
</tr>
<tr>
<td>Eight-electrode</td>
<td>δₓ</td>
<td>0</td>
<td>0</td>
<td>−200</td>
<td>N/A</td>
</tr>
</tbody>
</table>

50.8 mm, thickness 0.66 mm, and outer diameter 9.5 mm. ANSYS workbench with the PiezoAndMEMS extension is used to conduct the FE modeling as shown in Fig. 4. For the conventional tube, the length of the outer circumferential Z-electrode is one-third of the length, and the quadrant electrodes are two-thirds of the length. An aluminium holder which serves as a sensor target in experiments is also modeled. Table 1 lists the piezoelectric material properties in stress form (ε). A cylindrical co-ordinate system is used to define the polarization vector, which is oriented radially inward. Input voltages are applied to the three tube actuators as illustrated in Fig. 1. Table II lists the actuation voltages applied to each electrode configuration.

FE simulation results are summarized in Table III. The full-length configuration exhibits an 18% increase in lateral scan range and 52% increase in vertical scan range compared to the conventional electrode configuration. The normalized cross-couplings, φ/δₓ and δᵧ/δₓ, are also increased by about 30% and 35%, respectively, primarily due to the increase in the tilt angle and a larger strain experienced by the tube.

Table III also reports the vertical travel range per mm of vertical electrode (δᵧ/Lᵧ). Since the full-length and eight-electrode configurations are limited to negative voltages on the internal electrode, the travel range per mm of electrode length is half that of the conventional tube. However, since the effective electrode length of the full-length and eight-electrode configurations is longer, the overall vertical travel range is greater (assuming the vertical electrode length is less than half the tube length).

For the eight-electrode tube, the lateral scan range is reduced by 49% and 57% compared to the conventional and full-length tube, respectively. However, the eight-electrode tube shows negligible vertical and tilting motion induced by lateral deflection. The vertical scan range of the eight-electrode tube is also increased by 52% compared to the conventional tube due to the driven internal electrode.

Since the electrode configurations do not alter the resonance frequencies or mode shapes [22], they are not studied in this work. However, it can be noted that eliminating the circumferential electrode can reduce the tube length and increase resonance frequency [22].

**IV. EXPERIMENTS**

Fig. 5 shows the experiment setup for displacement measurement of the three tubes. Two MicroSense 6810 capacitive sensors are used to measure the vertical displacement δᵧ and the tilt angle φ. A MicroSense 4810 capacitive sensor is used to measure the lateral deflection δₓ. All three sensors have a sensitivity of 10 μm/V. The bandwidth of the three sensors are...
TABLE III

|   | Analytical, FE, and Experimental Results Comparing the Maximum Deflection and Cross-Coupling of the Three Electrode Configurations |
|---|---|---|---|---|---|---|---|
|   |   |   |       |       |       |       |       |       |       |       |       |       |
| X | δx (μm) | ±18.1 | ±20.3 | ±10.1 | ±22.35 | ±24.0 | ±10.1 | ±26.24 | ±42.4 | ±14.73 |
|   | φ (rad) |  |  |  |  |  |  |  |  |  |  |  |
|   | δz (μm) |  |  |  | ±507.07 | ±763.02 | ±27.56 | ±740.6 | ±1486.7 | ±17.1 |
|   | φ/δx (rad/m) |  |  |  |  |  |  |  |  |  |  |  |
|   | δz/δx (×10⁻³) |  |  |  |  |  |  |  |  |  |  |  |
| Z | δx (μm) | ±1.41 | -4.22 | -4.22 | ±1.31 | -3.8 | -3.8 | ±1.81 | -6.77 | -5.22 |
|   | δz/δx (μm/mm) | 0.167 | 0.0831 | 0.0831 | 0.154 | 0.0748 | 0.0748 | 0.213 | 0.133 | 0.103 |

Fig. 6. Measured deflections, δx, and δz, for the conventional, full-length, and eight-electrode piezoelectric tube actuators.

set to 10 kHz. A PiezoDrive TD250 high-voltage amplifier with a gain of 25 V/V is used to drive the piezoelectric tube actuators. A dSPACE MicroLabBox prototyping system which has a sampling rate of 80 kHz are used to generate the input signals and records the sensor measurements. To generate X-displacement, a 1-Hz sinusoidal signal is amplified to ±200 V. For both the eight-electrode and full-length tube actuators, negative voltages in the range of −200 to 0 V are applied to their inner electrode to produce vertical displacement. For the conventional tube, the circumferential Z-electrode is driven with ±200 V while keeping the internal electrode at ground to produce Z-displacement.

The measured displacement and cross-coupling of the three tubes is compared in Table III and plotted in Figs. 6 and 7. Compared to the conventional electrode configuration, the full-length electrode configuration exhibits a 62% increase in the lateral scan range and a 87% increase in the vertical scan range. The normalized cross-couplings φ/δx and δz/δx are also increased by 24% and 41%, respectively, as there are proportional to the lateral range.

For the eight-electrode configuration, the lateral scan range is 44% less than the conventional configuration. However, the normalized tilting φ/δx and vertical cross-coupling δz/δx are reduced by 96% and 43%, respectively. The proposed actuation method increases the δz range by 44% compared to that of the conventional electrode configuration. Although the eight-electrode configuration has the same length as the full-length configuration, there is a discrepancy in the measured δz due to different inner electrode lengths caused by manufacturing imperfections.

The hysteresis of the conventional, full-length, and eight-electrode actuators in the X-axis is 20.4%, 13.5%, and 17.5% of the full scan range, respectively. The hysteresis exhibited in the Z-axis is 22%, 15.8%, and 14.7%, respectively. Reduction of hysteresis can be achieved by either open-loop [23], [24] or closed-loop methods [25], [26].

Fig. 7. Measured cross-coupling motions from X to φ and from X to Z.
The discrepancies between the simulated and experimental results are partially due to uncertainty in $d_{31}$. Piezoelectric constants are estimated for small-signals and do not account for the hysteresis nonlinearity observed in Fig. 6. Significant differences in $d_{31}$ are expected when the full voltage range is utilized [27]. The $d_{31}$ value of the full-length configuration was found to increase from 305 to 440 pm/V when the tube is driven at $-10$ and $200$ V, respectively.

V. CONCLUSION

This article proposed two new methods for driving piezoelectric tube actuators. The first method aims to maximize the lateral and vertical deflection by driving the internal electrode, which eliminates the need for a circumferential Z-electrode. Experimental results show a 62% increase in lateral scan range and an 87% increase in the vertical scan range.

A second configuration is also described with eight external electrodes and a driven internal electrode. This method is primarily aimed at eliminating the vertical motion and tilting induced by lateral deflection. Experimental results show a 96% and 62% reduction in tilting and vertical cross-coupling, respectively, and 44% increase in vertical scan range. However, the lateral scan range was also reduced by 44%.

The proposed eight-electrode configuration with driven internal electrode is recommended for applications that require maximum vertical scan range with lowest possible tilting and vertical cross-coupling. For applications where tilting is not a concern, the proposed full-length tube actuator is recommended.

REFERENCES


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